

# A THREE-DIMENSIONAL KINEMATIC ANALYSIS OF THREE KICKING TECHNIQUES IN FEMALE SOCCER PLAYERS

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Human movement is a highly complex phenomenon that involves the interaction of a number of segments, muscles, and articulations of the human body. The motion of one segment will influence the motion of an adjacent segment because of the linked nature of the human body. Hudson (1986) suggested that a definite sequence and timing pattern must exist between these segments for successful performance to exist. How the segments interact and the timing pattern used during a movement is not well understood.

Kicking is a basic skill used in a variety of sport activities. Putnam (1983) has indicated that one component of kicking a ball is a correctly timed sequence of body segments. The sequence of segmental rotations for a kick has been labeled sequential with initial rotation at the pelvis, followed by the thigh, leg, and foot segments rotating about their respective axes. The soccer instep kick has been identified as a three-dimensional kicking motion (Huang, Roberts, & Youm, 1982), however, no research was found to validate this statement. Within a kicking pattern, various mechanical parameters may remain invariant despite a change in the purpose of the kick. Phillips (1985) stated that variability in some biomechanical parameters and invariance in others could aid in our understanding of the interrelationships between mechanical variables.

The specific purposes of this study were: (a) to describe the timing, sequence, and interaction of segments in a three-dimensional motion of a three-segment system, and (b) to investigate the invariance of mechanical parameters associated with three different soccer instep kicks.

## METHODOLOGY

Seven female Division I intercollegiate soccer players volunteered as subjects. Demographic **data on** subjects (age:  $20.1 \pm 1.5$  yrs; weight:  $61.1 \pm 2.8$  kg; height:  $151.8 \pm 3.1$  cm) were consistent with **data** found in the literature. **Anthropometric data were** obtained and 18 markers placed on specific bony landmarks of **each** subject for **ease** of analysis. Subjects were filmed from a  $60^\circ$  angle of convergence with two 16 mm high-speed cameras (LOCAM and PL-1) operating **at** nominal frame rates of 200 **frames/sec**. Subjects **performed** 2 practice trials followed by 2 mals of 3 different **kicks** (low drive, high drive, and maximum distance). The three kicks were filmed in random order by subject

Prior to filming of the subjects, a **control** object was filmed for application of the Direct Linear **Transformation (DLT)** method of three-dimensional (**3D**) analysis. After **the films** were processed, a NAC analysis film projector, Numonics Graphic Digitizer (2200), **Packard** Bell PC computer, and software (**Zimmerman**, 1989) were used in digitizing 18 **data** points. Data files were synchronized with the computer program SYNC (**Yu**, 1990). The synchronized **x,y** coordinates were entered into the DLT program to generate **x,y,z** coordinates. A second-order **Butterworth** digital filter (Winter, 1979) was used to smooth **the displacement data**. Instantaneous values for velocity and acceleration were calculated by the First Central Finite Difference Technique. A 3D model of the **kicking leg** was constructed with **vector** and mamx algebra to analyze the segmental angular displacements about the pelvis, hip, and **knee** of the kicking leg (see Figure 1). Information about the model can be found in **Tant** (1990).

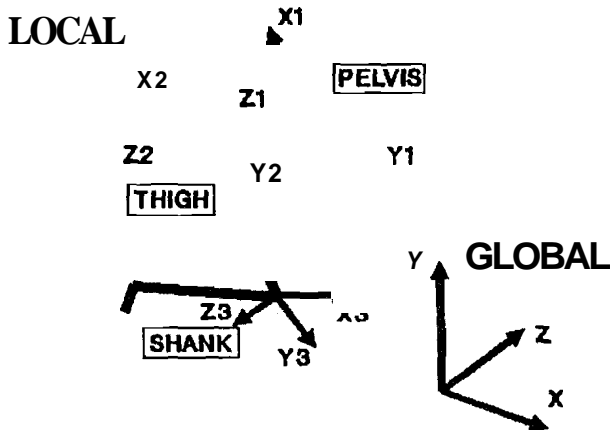


Figure 1. Three-segment lower body model

Temporal periods relative to **joint** action, timing delays between adjacent segments, and percentages of shared positive **contributions** between adjacent segments were investigated to **determine** segmental interactions.

## RESULTS

Huang et al. (1982) suggested that considerable rotation of the pelvic girdle might occur during a 3D soccer instep kick. As seen in Table 1, range of motion (ROM) for pelvic rotation (PLR) varied from 18.3 degrees for the low drive (LD) and maximum distance (MD) kicks to 13.2 degrees for the high drive kick (HD). Increased hip flexion and extension (HFE) and knee flexion and extension (KFE) was noticed during the HD kick. Hip abduction and adduction (HAB) remained consistent among the three kicks. Decreased total time (TTM) and increased resultant ball velocities (RBV) were found during the low drive and maximum distance kicks.

Table 1  
Angular Displacements of Three Soccer Instep Kicks

Variable	LD		HD		MD	
	<u>M</u>	<u>SD</u>	<u>M</u>	<u>SD</u>	<u>M</u>	<u>SD</u>
PLR (°)*+	18.3	3.5	13.2	5.2	18.3	4.7
HFE (°)*	37.8	5.7	57.9	3.9	45.9	2.8
HAB (°)	19.1	3.1	18.3	2.1	17.2	2.9
KFE (°)*+	74.5	4.3	94.5	4.0	70.7	3.8
TTM (ms)*	152.0	2.3	165.0	3.5	158.0	2.7
RBV (m/s)*+	17.01	3.5	13.51	6.6	16.17	2.8

\*  $p < .05$  HD vs. LD +  $p < .05$  HD vs. MD

A one-way ANOVA with repeated measures revealed several significant differences between the angular displacements of the 3 kicks. A Tukey post-hoc analysis indicated that PLR, HFE, KFE, TTM, and RBV were different from the HD and LD kicks. Additionally, differences between the HD and MD kicks were noticed in PLR, KFE, and RBV.

A proximal to distal temporal segmental sequence, pelvis (PEL), thigh (THI), and then lower leg (LLG), was exhibited in all 3 kicks. The PEL and THI began forward motion simultaneously, approximately 2.8 ms delay for all kicks, as the LLG continued backward. A sequential delay was found between the PEL-LLG and the THI-LLG (between 70-77 ms delay) contributing to increased velocities. Between 15 to 25 ms prior to ball contact the PEL and THI slowed and the LLG continued to maximum angular velocity.

A one-way ANOVA with repeated measures revealed no significant differences ( $p < .05$ ) between the relative timing of the segments of each kick (see Figure 2). As shown in Figure 3 no significance was indicated between the relative timing of the 5 different phases of the kick (maximum thigh back, maximum shank back, support heel contact, ball contact, and ball release).

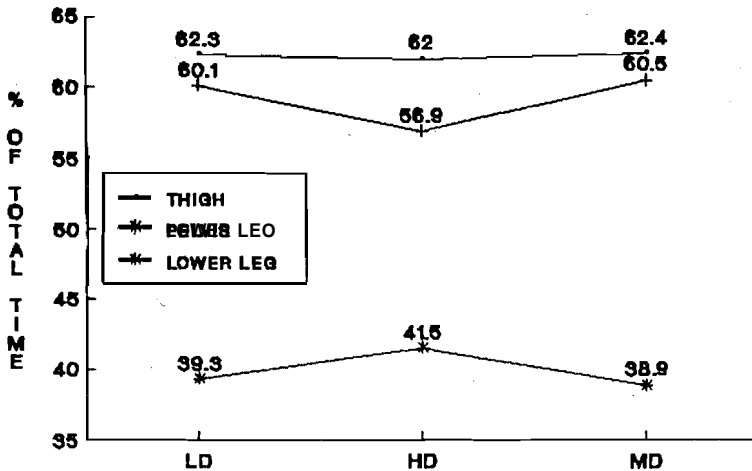


Figure 2. Relative timing of the segments

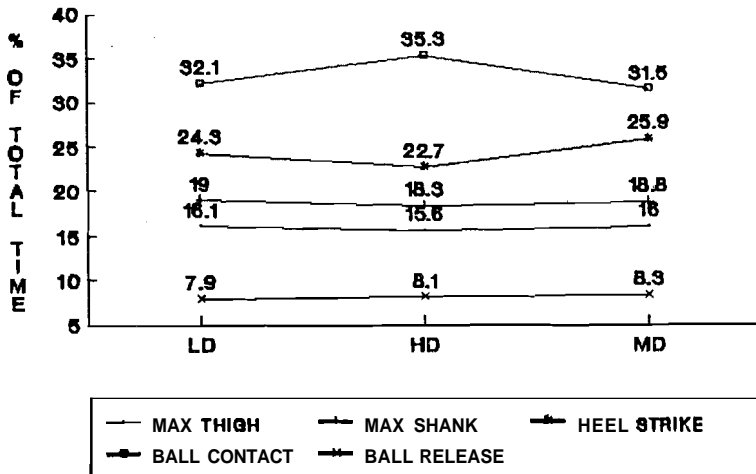


Figure 3. Relative timing of the phases

## DISCUSSION

The combination of increased **PLR** and a decrease in **HFE** and **KFE**, decreased the total movement time and produced the greatest resultant ball velocities. Female soccer players seemed to **take** advantage of increased pelvic width to **produce** maximum velocity. Small **delays** in timing and a **large** percentage of shared positive contributions indicated simultaneity between the **PEL** and **THI**. It appeared that the **PEL** and **THI** work as one unit to **initiate** the kick in a **pushlike** motion. A sequential pattern was observed between the **THI** and **LLG** because of large timing delays and small percentages of shared positive contributions. The soccer instep kick involves accuracy and velocity to produce a successful kick. The **PEL** and **THI** could aid in accuracy while the **THI** and **LLG** would generate maximum velocity. Because no significant differences were found in the relative timing of the segments it was found to be invariant indicating a common **temporal** structure for the soccer instep kick, regardless of type of kick.

## CONCLUSIONS

Very little is known about the patterns of coordination among the limbs which serve as the foundation of skilled movement. Invariance and variability within **biomechanical** parameters could provide information about interrelationships between mechanical variables of a **kicking** motion. For a **coach/teacher** of soccer, it appears that the **kicking technique** of the soccer instep kick could be taught with basic anatomical and mechanical concepts with slight **modifications based on** the specific purpose of the shot.

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